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Bianca Sousa Barros

Avaliação Isocinética do Músculo Deltoide Após
Artroplastia Invertida do Ombro /
Isokinetic Evaluation of the Deltoid Muscle After
Reverse Shoulder Arthroplasty

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Doutor João Bernardo Matos Nunes

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Isokinetic Evaluation of the Deltoid Muscle After Reverse Shoulder Arthroplasty

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COORDENADOR (se aplicável)

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É AUTORIZADA A REPRODUÇÃO INTEGRAL DESTA OBRA APENAS PARA EFEITOS DE INVESTIGAÇÃO, MEDIANTE DECLARAÇÃO ESCRITA DO INTERESSADO, QUE A TAL SE COMPROMETE.	<input checked="" type="checkbox"/>
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Dedico este trabalho à minha família e aos meus amigos que me apoiaram incansavelmente ao longo de todo o meu percurso.

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Isokinetic Evaluation of the Deltoid Muscle After Reverse Shoulder Arthroplasty

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Abstract

Background: Reverse Shoulder Arthroplasty depends on the Deltoid muscle to improve function and stability of the shoulder. Deltoid tension and pre- and postoperative conditions are key factors. Although good subjective results are reported, functional outcomes have shown variable improvements. The purpose of this study is to understand the biomechanical and functional influence of the Reverse Shoulder Arthroplasty in the Deltoid.

Methods: Fifteen participants after unilateral Reverse Shoulder Arthroplasty, were evaluated with isokinetic dynamometer (Abduction/Adduction and Forward Flexion/Extension), Electromyography and Constant-Murley Score. The arm without the prosthesis was considered the best performance status and used as comparison. Arm-length was measured and calculated the difference between arms. Participants were divided in two groups according to Constant-Murley Score of the arm without prosthesis: Group 0 (superior/equal to 80) and Group 1 (inferior to 80).

Findings: Significant differences in isokinetic parameters were observed, especially in Group 0, with the arm without prosthesis having better results. The Electromyography showed that Group 0 has an overall decrease of the electromyography activity in the arm with prosthesis, especially in the anterior and middle portion of the Deltoid, in Abduction and Forward Flexion. Group 1 revealed less significant differences.

Interpretation: Isokinetic evaluation combined with Electromyography is a useful tool to assess muscular and joint outcomes. This study demonstrated that Reverse Shoulder Arthroplasty has a significant effect in range of motion and strength of the shoulder joint and the Deltoid. Shoulders with the prosthesis presented worse performance, but these changes may only be significant when a higher functional level is present.

Key words: Deltoid, Reverse Shoulder Arthroplasty, Isokinetic, surface electromyography

1. Introduction

Reverse Shoulder Arthroplasty (RSA) depends on the deltoid muscle to improve function and stability of the shoulder joint, using a convex glenoid and a concave humeral component. Since Paul Grammont's concept of medializing and lowering the center of rotation of the cuff-deficient shoulder (Grammont et al., 1987), its use has been expanded to other pathologies (Jazayeri and Kwon, 2011).

The concept of RSA consists in a joint with a fixed center of rotation on the scapula and a cup on the humerus to provide a stable fulcrum. This fulcrum prevents superior humeral head migration and allows the elevation of the arm performed by the Deltoid, despite the absence of rotator cuff muscles (Hamilton et al., 2015).

With expanding indications for RSA, understanding the effect on the surrounding soft-tissues may be useful to improve the results and prevent failures. Previous studies concluded that there is a medial translation of the humerus compared to its original anatomy and shortening of the remaining rotator cuff (Ackland et al., 2015).

Deltoid tension is modified by the new center of rotation (Hamilton et al., 2013), and is paramount to the success of RSA. Its role is also critical to avoid dislocation and failure to adequately tension the Deltoid may result in prosthetic instability, which is one of the most significant complications (Lädermann et al., 2014).

Pre- and postoperative conditions of the Deltoid are key factors for the surgical outcome as arm elevation is mostly dependent on this muscle after RSA (Boudreau et al., 2007). An excessive lengthening in the Deltoid can be associated with neurologic lesions, restricted motion with fixed arm abduction, acromial or scapular spine fractures. On the other hand, an insufficient tension of this muscle may be associated with postoperative poor anterior elevation and prosthetic instability (Lädermann et al., 2014). Optimal conditions of the Deltoid may be difficult to assess pre and intra-operatively. As such, surgeons have to select the correct size and/or combination of RSA implants based mostly on experience, in order to achieve tension and stability in replaced joints (Hatta et al., 2016).

Although RSA is a good solution in cases of rotator cuff deficient shoulders, resulting in good subjective results, functional outcomes have shown variable improvements in the range of motion. Poor postoperative forward flexion can be associated with improper use, poor preoperative forward flexion, poor patient selection and postoperative complications (such as dislocation, spine scapula fracture or neurologic impairment). These conditions may be caused by inadequate Deltoid function, and the appropriate soft-tissue tension to provide the best functional outcome should restore arm length when compared with the contralateral arm (Lädermann et al., 2012, 2009).

The purpose of this study is to understand the biomechanical and functional implications in the Deltoid muscle after RSA.

2. Methods

2.1 Participants Selection

Surgical records were analyzed to retrieve patients submitted to unilateral RSA at a single institution, between September 2013 and September 2018. Inclusion criteria were defined as: 1) primary RSA through a deltopectoral approach, with a minimum 6 months of follow-up; 2) shoulder arthritis (primary or secondary), massive rotator cuff tears or proximal humerus fractures as diagnosis for surgery; 3) over 18 years-old; 4) willingness to participate and informed consent signing. Patients were excluded if they had previous surgery in the contralateral upper limb (including shoulder replacement), previous conditions that could influence humeral-length or side to side differences (such as humeral diaphyseal fracture), history of post-operative complications after RSA (neurologic injury, acromion, scapular spine or glenoid fractures, infection, instability or periprosthetic fractures), or if they missed the required evaluations. The institutional ethics committee approved the research protocol and all participants gave their written informed consent before the evaluation.

2.2. Measurements

All measurements were performed in LABIOMEPE – Porto Biomechanics Laboratory, evaluating one participant at the time and in a single evaluation. The contralateral arm was defined as control-group for comparison.

The Constant-Murley Score (CMS) was assessed for each shoulder. Range of Motion (RoM) in active forward flexion and abduction was evaluated using a goniometer, with its axis placed over the joint and determining the number of degrees from neutral position with the arm at the side (Hayes et al., 2001).

Humeral length was measured using an anthropometer, from the acromial to the radial external landmarks, as indicated in Figure 1. Each arm was measured twice, and the mean value of measurements was used for analysis (International Society for the Advancement of Kinanthropometry (ISAK), 2001).



Figure 1: The participant assumed a relaxed standing position with the arms hanging by the side and the measure is from the acromiale landmark ("A"), the point on the superior part of the acromion border in line with the most lateral aspect, to the radiale landmark, the point at the proximal and lateral border of the head of the radius ("B").

The isokinetic evaluation combined with electromyography (EMG) was performed lastly. The isokinetic evaluation used the Biodex System 4 Pro, an isokinetic dynamometer for muscle function with fully assisted dynamometer height adjustment, front-to-back chair adjustment and side-to-side adjustment. This isokinetic dynamometer provides a constant velocity with accommodating resistant throughout a joint's RoM. This resistance is provided at a user-defined constant speed ("Biodex System 4 Pro Specifications," 2020). The dynamometer velocity was 60 degrees per second. In all exercises, participants were stabilized in the chair with shoulder and abdominal straps. The position of the chair, in height, front-to-back and side-to-side position, was adapted to every participant so that the anatomical center of the shoulder joint was aligned to the dynamometer axis.

There were four different protocols in the Biodex: isometric exercise at abduction, isometric exercise at forward flexion, isokinetic exercise with abduction/adduction, and isokinetic exercise for forward flexion/extension. For the abduction/adduction protocol, the dynamometer was set with 10-degree tilt. However, for the forward flexion /extension protocol the dynamometer was set in neutral tilt (0 degrees). The isometric exercises were at 45 degrees in abduction and forward flexion, executing two contractions separated by one-minute rest. The isokinetic exercise consisted in five repetitions of full ROM movements, with an interval of 0 degrees and 135 degrees, both for abduction/adduction and forward flexion /extension. The participant started with the arm not submitted to RSA and did every exercise with that arm first and then with the arm with prosthesis. Before each exercise, isometric and isokinetic, the participant was asked to try to do the exercise as a warm-up, followed by a five minutes rest before the exercise for record was performed. The order of exercises was: 1) isometric in abduction; 2) isokinetic with abduction/adduction; 3) isometric in forward flexion; 4) isokinetic in forward flexion/extension. The participants were encouraged to reach the maximal muscle and joint performance during all exercises. The following parameters were extracted for further analysis: Peak Torque, Peak Torque per Body Weight (PT/BW), Angle of Peak Torque (AngPT) in degrees, Power in Watts and Work in joules.

In addition, surface electromyography was used simultaneously with the isokinetic evaluation of the three portions of the Deltoid muscle (anterior, middle and posterior), during the abduction/adduction and forward flexion /extension exercises. Surface bipolar EMG electrodes (Dormo&Blaico SX-30, Telic S.A. Spain) were placed on the skin above the Deltoid according to the Surface Electromyography for the Non-Invasive Assessment of Muscles recommendations and with an inter-electrode distance of 20 mm (SENIAM, 2019). The skin was cleaned with a cotton swab soaked in 90% alcohol prior to electrode's placement. The EMG signals were bandpass filtered (5-500 Hz), amplified and recorded with a BIOPAC MP100 (BIOPAC Systems, INC, USA) analog-to-digital converter operating at a 2000Hz sampling frequency. A custom written Matlab R2014a (MathWorks, MA, USA) routine was used to process the EMG data. The isokinetic dynamometer RoM was used to set four performance ranges: 0-45°, 45-90°, 90-135° 135-180°. The EMG envelopes was then normalized to its maximum value of each range, and

the average muscle activation in each range was extracted. As such, Deltoid muscle activity was recorded while the undertaking the exercises in the isokinetic evaluation.

2.3. Statistical analysis:

Statistical Analysis was performed using IBM SPSS Statistics software (IBM Corporation, NY, USA). All data are expressed as means \pm standard deviation (SD). The Wilcoxon test was used to assess differences between the shoulder with RSA and the shoulder without RSA in the parameters analyzed. The probability level $p < 0.05$ was defined as statistically significant.

3. Results

The study included 15 participants (13 women and 2 men). The mean age was $66,53 \pm 6,23$ years (range from 52 to 78). Eleven participants had surgery in the right shoulder and four in the left shoulder. The indications for RSA were degenerative (Primary and Secondary Arthritis) and traumatic causes. The mean time between surgery and the evaluation was $31,67 \pm 16,64$ months (range from 9 to 67 months).

In all statistical analysis showed below, the differences were calculated between the arm with RSA, designated by "Ipsilateral", and the arm considered healthy, without RSA, designated by "Contralateral".

3.1. Constant-Murley Score

Constant-Murley Score (CMS) was compared for each arm (Table 1). Side-to-side comparison of the CMS revealed that Ipsilateral shoulders had a mean CMS of $52,7 \pm 10,57$, compared to $77,76 \pm 8,57$ of the Contralateral side ($p < 0,001$).

From the 15 participants, 13 referred no pain in Contralateral arm. In the Ipsilateral arm, 9 participants referred minor pain and 3 no pain, with only 3 referring moderate pain. In Abduction, 10 of the participants had a RoM of $121 - 150^\circ$ in the Contralateral arm (4 had a RoM of $91 - 120^\circ$ and 1 had $>151^\circ$). However, in the Ipsilateral arm, 9 participants had a RoM of $91 - 120^\circ$ for Abduction, 4 had $61 - 90^\circ$ and 2 had a higher RoM of $121 - 150^\circ$. In Forward Flexion, the same tendency between arms was observed: 12 participants achieved the interval of $121 - 150^\circ$ in the Contralateral arm (two $91 - 120^\circ$ and one $>150^\circ$). In the Ipsilateral arm, 7 achieved a RoM in the interval $91 - 120^\circ$, five at $61 - 90^\circ$ and 3 at $121 - 150^\circ$. In External Rotation, all 15 participants had the maximum classification (10) for the Contralateral arm. However, for the Ipsilateral results were variable ranging from 2 to 10. In Internal Rotation, 14 participants had 10 of classification (one participant had 8) in the Contralateral arm. In the Ipsilateral arm, 2 participants had a classification of 0, 6 a classification of 2, 2 had a classification of 6 and 5 had a classification of 8. The mean difference between arms in strength is 2,04 kg.

The participants were divided in two groups based on the CMS of the arm without RSA. Therefore, the statistical analysis was performed in one group with 6 participants with CMS superior or equal to 80, designated by Group 0, and another group with 9 participants with CMS inferior to 80, designated by Group 1.

3.2. Arm length

Mean arm length was $28,56 \pm 2,24$ cm in the Ipsilateral arm, comparing with $27,21 \pm 1,69$ cm in the Contralateral one, indicating a mean difference of $1,35 \pm 0,96$ cm ($p=0,07$)

Participants in group 0 had a longer arm length in the Ipsilateral side, with a mean difference of $1,54 \pm 1,10$ cm ($p=0,22$). Participants in Group 1 also demonstrated an Ipsilateral arm $1,22 \pm 0,91$ cm (mean) longer than the Contralateral ($p=0,19$).

3.3. Isokinetic Dynamometer Evaluation

In the Isokinetic Dynamometer Evaluation the following parameters were evaluated: Peak Torque in Newton meters (T/BW (N.m)), Peak Torque per Body Weight (PT/BW (%)), Angle of Peak Torque in degrees (AngPT (Deg)), Power in Watts (Pow(W)) and Work in Joules (Work (J)).

3.3.1. Peak Torque (T/BW):

In terms of Peak Torque in Abduction/Adduction isokinetic exercise, Group 0 had significant differences between shoulders in Abduction as the Ipsilateral side was significantly lower ($p=0,043$). In Group 1, no significant differences between arms were found. Peak Torque in Adduction did not demonstrate significant differences between Ipsilateral and Contralateral sides, both in Group 0 and 1.

In Forward Flexion/Extension isokinetic exercise, Group 0 also demonstrated that Peak Torque was significantly lower in the Ipsilateral side both in Forward Flexion ($p=0,043$) and Extension ($p=0,043$). In Group 1, Peak Torque in the Ipsilateral side was significantly lower in Extension ($p=0,015$). (Table 1 Suppl)

3.3.2. Peak Torque per Body weight (PT/BW), Time of Peak Torque (TimePT), Angle of Peak Torque (AngPT), Power and Work:

In the Abduction/Adduction isokinetic exercise, in Group 0, the Ipsilateral shoulder had significantly lower results regarding PT/BW in Adduction ($p=0,043$), Power in Abduction and Adduction ($p=0,043$ for both) and Work in Abduction and Adduction ($p=0,043$). All the other evaluated parameters were not significantly different between sides.

In group 1, there were no significant differences between sides except in the AngPT in Abduction, which was lower in the Ipsilateral shoulder ($p=0,021$). (Table 2 Suppl)

Forward Flexion/Extension isokinetic evaluation demonstrated that in Group 0, the Ipsilateral shoulder was significantly lower in PT/BW in Forward Flexion and Extension ($p=0,043$ for both), AngPT in Extension ($p=0,043$), Power in Forward Flexion and Extension ($p=0,043$ for both), Work in Forward Flexion and Extension ($p=0,043$ for both).

In Group 1, the Ipsilateral shoulder had significantly inferior values of PT/BW in Extension ($p=0,015$), AngPT in Forward Flexion ($p=0,015$), and Work in Extension ($p=0,038$). No other side-to-side differences were found in the remaining parameters. (Table 3 Suppl)

3.4. Electromyography

3.4.1. Anterior, Medial and Posterior Deltoid, in Abduction/Adduction:

In Group 0, electromyographic assessment of the Anterior Deltoid highlighted significant differences between shoulders in the following movements and range of performances: Abduction in 90 - 135° ($p=0,043$), Adduction in 90 - 135° ($p=0,043$) and in 0 - 45° ($p=0,043$).

In the Middle Deltoid portion, significant side to side differences were found in Abduction in 0 - 45° ($p=0,043$) and in 90 - 135° ($p=0,043$), and Adduction in 90 - 135° ($p=0,043$).

In terms of the Posterior portion of the Deltoid muscle, the parameters with significant differences are Abduction in 0 - 45° ($p=0,043$) and Adduction in 90 - 135° ($p=0,043$).

The Mean Torque (MT) also had significant differences between the shoulders in Abduction in 45 - 90° ($p=0,043$) and in 90 - 135° ($p=0,043$), Adduction in 90 - 135° (p of 0,043), in 45 - 90° ($p=0,043$) and in 0 - 45° ($p=0,043$). The Maximum Torque (Tmax) had significant differences in Abduction and Adduction ($p=0,043$ for both).

Group 1 demonstrated statistically significant differences between shoulders in Adduction in 0 - 45° ($p=0,015$) for the Middle portion of the Deltoid muscle.

All statistically significant differences mentioned above are related to a higher electric activity in the Contralateral shoulder, except for two parameters in Group 0: Anterior Deltoid in Adduction in 90 - 135° and for the Middle portion of the Deltoid in Adduction in 0 - 45°, where the arm submitted to RSA had higher activity. (Tables 4, 6 and 8 Suppl)

3.4.2. Anterior, Middle and Posterior Deltoid, in Forward Flexion/Extension:

In the Anterior Deltoid, Group 0 had significant differences between shoulders in Forward Flexion in 0 - 135° ($p=0,043$).

In the Middle portion of the Deltoid muscle, there were significant differences in Forward Flexion in 90 - 135° ($p=0,043$).

The MT also had significant differences in Forward Flexion in 0 - 45° ($p=0,043$), in 45 - 90° ($p=0,043$), in 90 - 135° ($p=0,043$), and in Extension in 90 - 135° ($p=0,043$), in 45 - 90° ($p=0,043$) and in 0 - 45° ($p=0,043$).

Group 1 had significant differences between shoulders in terms of MT in Forward Flexion in 90 - 135° ($p=0,012$), in Extension in 45 - 90° ($p=0,012$) and in 0 - 45° ($p=0,012$). The Tmax was also significant better in the Contralateral arm in Extension ($p=0,015$).

Once again, all statistically significant differences mentioned above are related to a higher electric activity in the arm not submitted to RSA in both groups. (Tables 5, 7 and 9 Suppl)

4. Discussion

The purpose of this study was to evaluate the implications of RSA in the Deltoid muscle function, using its isokinetic profile and electromyography data. Isokinetic muscle tests are not frequently used in clinical practice, especially when associated with EMG, which results in limited literature available. The understanding of the biomechanics of the reverse shoulder anatomy is crucial, although there are few studies regarding the individual properties of the Deltoid adaptation after RSA (Fischer et al., 2019; Rugg et al., 2019; Walker et al., 2016). Most studies mainly evaluate isometric muscle strength. However, most functional activities are dynamic which makes imperative to have an isokinetic evaluation that can be related to functional and clinical outcome (Alta et al., 2014, 2012).

From a clinical standpoint, this study demonstrated that CMS in RSA shoulders were lower than the contralateral side, but as no baseline data were available, this may also result from a worse pre-operative overall function. In fact, pre-operative RoM appears to have a great influence in post-operative RoM (Friedman et al., 2019). Although pain level was very similar for both sides, RoM in Abduction and Forward Flexion were decreased in the RSA shoulder, as well as the strength assessed in the CMS. It is important to notice that the expectation for functional and RoM results have to be set case-by-case, depending on the pathology indicative for RSA, the performance status and the possibility of rehabilitation for the Deltoid and periscapular musculature (Boudreau et al., 2007). There is an overall RoM decreased in RSA shoulders comparing to healthy controls but these differences may not be as important clinically, as an acceptable RoM is achieved and pain relief is significant. In fact, RSA seems to be effective in pain relief and allows a satisfactory functional outcome (Jeon and Rhee, 2018), even though pre-lesion function seems not achievable, as we found in our study. In addition, a previous study suggests that the limited RoM after RSA can be a result of lack of joint torque generation (Bergmann et al., 2008), showing the importance of an isokinetic evaluation.

In this study, the contralateral arm was defined as the control for comparison. Because of the exclusion criteria, the contralateral arm should be the best performance status for each participant, as all individuals who had had any history of previous or current shoulder pathologies

and surgeries were excluded, as it could interfere with its strength and RoM. According to Constant et al, the cut-off value of 80 points in the CMS is considered as a normal result in the age range of this sample (Constant et al., 2008). Based on this, we attempted to identify objective isokinetic side-to-side differences in participants that had higher contralateral shoulder function (Group 0, CMS superior or equal to 80) and those with lower contralateral function (Group 1, CMS inferior to 80). Overall, patients in Group 0 demonstrated more statistically significant differences between shoulders, with the contralateral arm having a better isokinetic and EMG performance than the RSA one.

Isokinetic evaluation enables a safe, objective and reliable assessment of muscular performance. It provides a dynamic measurement of isolated joint motions and muscular contributions, and helps to assess underlying muscular strength and strength balance (Ellenbecker and Davies, 2000). As previous studies using isokinetic evaluation in samples with similar mean age and evaluating abduction/adduction and/or forward flexion/extension, we used dynamometer velocity set of 60 degrees per second (Alta et al., 2012; Wang et al., 2016). All participants were able to execute the exercises, which reveals as an appropriate velocity.

In this study, patients in Group 0 demonstrated higher Peak Torque in Abduction, Forward Flexion and Extension in the contralateral shoulder, but in patients with lower contralateral function, only Peak Torque in Extension was significantly affected. Deltoid muscle is mostly responsible for abduction, with a role in forward flexion by assisting Pectoralis Major in drawing the arm forward and with a minor role in extension by assisting Latissimus dorsi and Teres Minor (Susan Standing DSc, 2016). After RSA, the lever arm of the Deltoid is improved so that Forward Flexion and Abduction can be achieved without the stabilizing role of the rotator cuff (Boudreau et al., 2007). Our findings suggest that although RSA appears to decrease the maximum strength of the Deltoid, this may only be significant in patients with a higher than normal overall shoulder function. A previous study showed that pre-operative shoulder strength and RoM have a major role in the post-operative outcome, as individuals with poor function previous to the prosthesis will have worse functional outcomes with RSA (Li et al., 2020).

Other parameters of the isokinetic evaluation also revealed this tendency, that more significant differences were only reached when a higher contralateral function was present. In the scapula plane, several parameters (PT/BW, Work, Power) were significantly lower in the RSA, both in Abduction and Adduction, but only in Group 0. Group 1 demonstrated lower Angle of PT in Abduction in the RSA shoulder, pointing out that the maximum strength generation is reached in a lower angle, and this holds even comparing with shoulders with poorer overall function. Nevertheless, this finding must be interpreted with caution, as no significant difference was found for the same parameter in Group 0, where side-to-side differences seem to be more aggravated. In the sagittal plane, many parameters were significantly decreased in the RSA shoulder of patients in Group 0 (PT/BW, AngPT, Power and Work), both in Forward Flexion and Extension. Group 1 also presented more significant differences in this plane, which may reveal that strength in the sagittal plane may be more significantly affected.

EMG analysis completed Deltoid evaluation and also demonstrated more significant side-to-side differences in Group 0. Deltoid electric activity in the Anterior and Middle portion was lower in the RSA shoulder, regarding Abduction and Forward Flexion in the 0-135° range, which is also consistent with the movements where Deltoid has a more important role (Fischer et al., 2019; Schwartz et al., 2013). This pattern was confirmed in the Mean Torque and in the Maximum Torque. Group 1 failed to demonstrate significant differences in the EMG, and this may represent that RSA can restore Deltoid electrical activity to levels similar to the contralateral shoulder in lower demand patients (with a lower overall shoulder function).

Alta et al. observed that participants with RSA have significant lower Torques in Abduction when compared to healthy subjects. Even though there are differences between this study and ours (such as the comparison with healthy participants versus using the contralateral arm and not specifically evaluation the Deltoid activity), these results corroborate our hypothesis that RSA does not totally restore shoulder's RoM and muscle strength (Alta et al., 2012). As mentioned before, there is very limited literature with studies that used similar protocols including isokinetic assessment complemented by EMG. This reveals as a limitation to have data to compare our findings and conclusions, as more studies using this kind of protocol are necessary.

RSA shoulders generally demonstrated a poorer isokinetic performance. Some studies highlighted that humeral length after RSA may influence Deltoid function due to slackening or fatigue induced by overtensioning (Lädemann et al., 2012; Li et al., 2020). In our study, humeral length was preserved after RSA, but there were significant differences in the isokinetic and EMG evaluation that may be conditioned by RSA design and surgical intervention.

This study has limitations that must be carefully interpreted. The limited number of participants may induce bias, and no baseline evaluation was available for comparison. However, isokinetic objective evaluation may be difficult before surgery, as many patients suffer from painful conditions that preclude an exhaustive functional assessment. Time elapsed from surgery was not homogenous between patients, and this may have an effect as some studies report a decrease in Deltoid function with time (Pegreffo et al., 2017). In addition, serial evaluation of this sample may contribute to the understanding of temporal effects and improve the reliability of assessment. In further studies, larger samples and standardized timings of evaluation would be more appropriate for improvement. The cut-off value of 80 for the CMS was used for separating two groups. The difference of mean CMS of each group was approximately 10 points, which may be argued that Group 0 did not have a clinically significant poor overall shoulder function of the Contralateral arm. Notwithstanding, this may be interpreted that RSA shoulders can achieve a nearly equivalent performance to the contralateral side if shoulder function is not severely decreased, but may fail to do so when function is exceedingly good.

5. Conclusion

Isokinetic evaluation combined with EMG is a useful and applicable tool to assess muscular and joint outcomes after RSA. This study demonstrated that this procedure has a significant effect in pain, RoM and strength of the shoulder joint and the Deltoid muscle. This effect was more relevant in patients with a better overall function of the contralateral shoulder, and may be only marginal when contralateral shoulders have a poorer function. In conclusion, isokinetic evaluation complemented with EMG and clinical scores (CMS) allowed us to have a more consistent and reliable understanding of the function of the Deltoid muscle after RSA.

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Tables

Table 1: Costant-Murley Score (CMS) for the arm with RSA designated by Constant_ipsi and the arm without RSA designated by Constant_contra. The bottom line shows the difference between CMS between arms.

	<i>Minimum</i>	<i>Maximum</i>	<i>Mean</i>	<i>Standard Desviation</i>
Constant_ipsi	37,54	70,67	52,729	10,56938
Constant_contra	61,50	91,83	77,7617	8,57314
Difference_CMS	4,38	48,58	25,0588	14,18078

Supplementary Material

Table 1 Suppl: “T/BW_Abd” – Peak Torque in Abduction, “T/BW_Add” – Peak Torque in Adduction, “T/BW_FF” – Peak Torque in Forward Flexion and “T/BW_E” – Peak Torque in Extension. There are presented values of mean \pm standard deviation, and values of z and p related to the Wilcoxon test performed to assess differences between the arm with RSA (“Ipsilateral”) and the arm without RSA (“Contralateral”), for Group 0 and Group 1.

		T/BW_Abd		T/BW_Add		T/BW_FF		T/BW_E	
Group 0	Ipsilateral	20,66 \pm 8,27	$z = -2,023$	3,72 \pm 0,78	$z = -1,826$	17,79 \pm 4,36	$z = -2,023$	9,44 \pm 6,58	$z = -2,023$
	Contralateral	33,45 \pm 12,87	$p = 0,043$	33,49 \pm 24,24	$p = 0,068$	40,03 \pm 13,72	$p = 0,043$	44,62 \pm 16,53	$p = 0,043$
Group 1	Ipsilateral	25,47 \pm 9,25	$z = -0,560$	12,14 \pm 17,47	$z = -0,770$	24,77 \pm 8,57	$z = -1,007$	17,44 \pm 19,86	$z = -2,429$
	Contralateral	24,36 \pm 6,40	$p = 0,575$	18,12 \pm 17,76	$p = 0,441$	29,62 \pm 13,97	$p = 0,314$	28,02 \pm 22,45	$p = 0,015$

Table 2 Suppl: Peak Torque per Body Weight (“PT/BW (%)”), Angle of Peak Torque in degrees (“AngPT (Deg)”), Power in Watts (“Pow(W)”) and Work in Joules (“Work (J)”) in Abduction and Adduction isokinetic exercise in group 0 and group 1. There are presented values of mean \pm standard deviation for the arm with RSA (“Ipsi”) and the arm without RSA (“Contra”), and values of z and p related to the Wilcoxon test performed to assess differences between arms.

		Abduction				Adduction			
		Mean \pm SD (Ipsi)	Mean \pm SD (Contra)	Z	p	Mean \pm SD (Ipsi)	Mean \pm SD (Contra)	Z	p
PT/BW (%)	Group 0	25,38 \pm 10,80	34,82 \pm 12,27	-0,674	0,500	16,94 \pm 14,47	36,97 \pm 24,36	-2,023	0,043
	Group 1	26,10 \pm 8,32	24,98 \pm 8,67	-0,770	0,441	17,01 \pm 15,33	18,51 \pm 10,53	-0,356	0,722
TimePT (Msec)	Group 0	1300,00 \pm 894,37	693,33 \pm 341,51	-1,214	0,225	1984,00 \pm 664,36	2071,67 \pm 838,80	-0,674	0,500
	Group 1	1271,11 \pm 1201,40	1670,00 \pm 557,54	-1,244	0,214	1738 \pm 803,70	1983,33 \pm 736,27	-0,652	0,515
AngPT (Deg)	Group 0	61,40 \pm 21,87	48,67 \pm 16,70	-0,944	0,345	14,20 \pm 7,79	38,33 \pm 39,47	-0,730	0,465
	Group 1	56,56 \pm 23,43	91,78 \pm 23,73	-2,310	0,021	32,56 \pm 28,57	36,11 \pm 24,89	-0,830	0,407
Pow (w)	Group 0	6,08 \pm 3,61	14,88 \pm 6,62	-2,023	0,043	0,14 \pm 0,11	11,53 \pm 11,33	-2,023	0,043
	Group 1	8,57 \pm 4,37	7,88 \pm 2,58	-0,770	0,441	2,26 \pm 4,09	3,60 \pm 5,00	-1,014	0,310
Work (J)	Group 0	52,72 \pm 23,28	199,78 \pm 80,16	-2,023	0,043	1,34 \pm 1,28	156,68 \pm 148,81	-2,023	0,043
	Group 1	95,42 \pm 56,95	104,69 \pm 48,13	-0,889	0,374	27,78 \pm 50,20	52,32 \pm 74,54	-1,007	0,31

Table 3 Suppl: Peak Torque per Body Weight (“PT/BW (%)”), Angle of Peak Torque in degrees (“AngPT (Deg)”), Power in Watts (“Pow(W)”) and Work in Joules (“Work (J)”) in Forward Flexion and Extension isokinetic exercise in Group 0 and Group 1. There are presented values of mean \pm standard deviation for the arm with RSA (“Ipsi”) and the arm without RSA (“Contra”), and values of z and p related to the Wilcoxon test performed to assess differences between arms.

		Forward Flexion				Extension			
		Mean \pm SD (Ipsi)	Mean \pm SD (Contra)	Z	p	Mean \pm SD (Ipsi)	Mean \pm SD (Contra)	Z	p
PT/BW (%)	Group 0	22,62 \pm 3,57	43,52 \pm 14,47	-2,023	0,043	14,08 \pm 4,25	47,40 \pm 19,48	-2,023	0,043
	Group 1	25,60 \pm 9,14	28,49 \pm 14,06	-0,533	0,594	17,56 \pm 15,54	26,91 \pm 15,69	-2,429	0,015
TimePT (Msec)	Group 0	1760,00 \pm 485,03	1555,00 \pm 578,472	-0,405	0,686	1430,00 \pm 257,59	940,00 \pm 459,35	-1,753	0,080
	Group 1	1610,00 \pm 1323,26	2306,67 \pm 1003,71	-1,481	0,139	1461,11 \pm 763,36	1571,11 \pm 868,99	-0,059	0,953
AngPT (Deg)	Group 0	96,60 \pm 21,63	101,17 \pm 38,47	-0,730	0,465	23,40 \pm 21,66	90,67 \pm 25,85	-2,023	0,043
	Group 1	68,44 \pm 22,96	105,11 \pm 30,90	-2,429	0,015	54,56 \pm 57,82	55,44 \pm 45,46	-0,356	0,722
Pow (w)	Group 0	6,86 \pm 2,80	19,33 \pm 8,69	-2,023	0,043	1,78 \pm 2,32	18,10 \pm 9,45	-2,023	0,043
	Group 1	8,93 \pm 3,58	10,08 \pm 5,56	-0,652	0,514	4,74 \pm 7,14	7,82 \pm 8,25	-1,863	0,063
Work (J)	Group 0	71,56 \pm 16,46	251,78 \pm 115,86	-2,023	0,043	20,76 \pm 31,94	238,88 \pm 123,02	-2,023	0,043
	Group 1	121,22 \pm 55,83	145,27 \pm 75,45	-1,244	0,214	64,70 \pm 95,05	106,94 \pm 111,45	-2,073	0,038

Table 4 Suppl: Differences between arms in the electromyographic assessment of the Anterior (DA), Middle (DM) and Posterior (DP) portions of the Deltoid Muscle during the Abduction/Adduction isokinetic exercise. Differences are represented by values of *z* and *p* related to the Wilcoxon test. It is also represented the values for the Mean Torque (“MT”) and the Maximum Torque (“Tmax”). Each parameter is evaluated for a specific interval of amplitude (0 - 45°, 45 - 90°, 90 - 135° and 135 – 180° in Abduction, and the reverse in Adduction).

		Abduction										Adduction												
		DA		DM		DP		MT		Tmax		DA		DM		DP		MT		Tmax				
		<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>			
Group 0	0 - 45°	-1,21	0,225	-	2,023	0,043	-	2,023	0,043	-	1,753	0,080	-	2,023	0,043	-	2,023	0,043	-	2,023	0,043	-	2,023	
	45 - 90°	-0,67	0,500	-	0,944	0,345	-	1,214	0,225	-	2,023	0,043	-	2,023	0,043	-	2,023	0,043	-	2,023	0,043	-	2,023	
	90 - 135°	-	2,023	0,043	-	2,023	0,043	-	1,826	0,068	-	2,023	0,043	-	2,023	0,043	-	2,023	0,043	-	2,023	0,043	-	2,023
	135 - 180°	-	1,604	0,109	-1,60	0,109	-1,60	0,109	-	1,342	0,180	-	-	-	-1,60	0,109	-1,60	0,109	-	1,342	0,180	-	-	
Group 1	0 - 45°	-	0,059	0,953	-	0,770	0,441	-	1,125	0,260	-	1,007	0,314	-	2,429	0,015	-0,770	0,441	-1,599	0,110	-1,599	0,110	-	-
	45 - 90°	-	0,770	0,441	-	0,770	0,441	-	0,533	0,594	-	1,207	0,204	-	-1,244	0,214	-0,770	0,441	-1,120	0,263	-0,059	0,953	-0,889	0,374

Table 5 Suppl: Differences between arms in the electromyographic assessment of the Anterior (DA), Middle (DM) and Posterior (DP) portions of the Deltoid Muscle during the Forward Flexion/Extension isokinetic exercise. Differences are represented by values of *z* and *p* related to the Wilcoxon test. It is also represented the values for the Mean Torque (“MT”) and the Maximum Torque (“Tmax”). Each parameter is evaluated for a specific interval of amplitude (0 - 45°, 45 - 90°, 90 - 135° and 135 – 180° in Abduction, and the reverse in Adduction).

		Forward Flexion										Extension									
		DA		DM		DP		MT		Tmax		DA		DM		DP		MT		Tmax	
		<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>	<i>z</i>	<i>p</i>
Group 0	0 - 45°	-0,677	0,498	-0,405	0,686	-0,944	0,345	-2,023	0,043	-2,023	0,043	-0,405	0,686	-0,135	0,983	-0,405	0,686	-2,023	0,043	-0,674	0,500
	45 - 90°	-1,483	0,138	-1,753	0,080	-0,944	0,345	-2,023	0,043			-1,214	0,225	-1,214	0,225	-0,135	0,893	-2,023	0,043		
	90 - 135°	-2,023	0,043	-2,023	0,043	-1,753	0,080	-2,023	0,043			-1,753	0,080	-0,674	0,500	-1,483	0,138	-2,023	0,043		
	135 - 180°	-1,000	0,317	-1,342	0,180	-1,342	0,180	-1,342	0,180			-	-	-1,342	0,180	-1,342	0,180	-1,342	0,180		
Group 1	0 - 45°	-0,296	0,767	-1,244	0,214	-1,599	0,110	-0,178	0,859	-1,007	0,314	-0,178	0,859	-0,415	0,678	-0,296	0,767	-2,192	0,028	-2,429	0,015
	45 - 90°	-0,889	0,374	-0,889	0,374	-0,178	0,859	-1,680	0,093			-0,533	0,594	-0,415	0,678	-0,296	0,767	-2,310	0,021		

Table 6 Suppl: Electromyographic results of the Anterior (DA), Middle (DM) and Posterior (DP) portions of the Deltoid Muscle in Group 0, in the Abduction/Adduction isokinetic exercise represented by values of mean and Standard Desviation (“SD”). It is also represented the Mean Torque (“MT”) and the Maximum Torque (“Tmax”). Each parameter is evaluated for a specific interval of amplitude (o - 45°, 45 - 90°, 90 - 135° and 135 – 180° in Abduction, and the reverse in Adduction).

		Abduction										Adduction									
		DA		DM		DP		MT		Tmax		DA		DM		DP		MT		Tmax	
		Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD
Contralateral	0 - 45°	0,75	0,18	0,76	1,37	0,68	0,06	20,80	9,89	23,50	8,96	0,11	0,03	0,21	0,10	0,22	0,15	12,88	11,30	23,63	16,83
	45 - 90°	0,91	0,14	0,88	0,08	0,88	0,19	21,57	8,77			0,13	0,08	0,21	0,13	0,24	0,15	20,56	15,55		
	90 - 135°	0,99	0,32	0,84	0,21	0,64	0,38	13,69	10,36			0,18	0,19	0,27	0,16	0,27	0,19	18,61	18,47		
	135 - 180°	0,43	0,39	0,43	0,37	0,42	0,38	5,96	8,08			-	-	0,16	0,15	0,14	0,12	11,40	14,98		
Ipsilateral	0 - 45°	0,65	0,12	0,59	0,09	0,53	0,13	8,72	4,92	14,86	6,47	-	-	0,24	0,09	0,21	0,08	0,25	0,20	2,09	1,32
	45 - 90°	0,87	0,21	0,81	0,19	0,65	0,40	0,37	0,83			0,26	0,13	0,31	0,08	0,28	0,06	0,24	0,44		
	90 - 135°	0	0	0	0	0	0	0	0			0,36	0,11	0	0	0	0	0	0		

135 - 180°	0	0	0	0	0	0	0	0			0	0	0	0	0	0	0		
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Table 7 Suppl: Electromyographic results of the Anterior (DA), Middle (DM) and Posterior (DP) portions of the Deltoid Muscle in Group 1, in the Abduction/Adduction isokinetic exercise represented by values of mean and Standard Desviation ("SD"). It is also represented the Mean Torque ("MT") and the Maximum Torque ("Tmax"). Each parameter is evaluated for a specific interval of amplitude (0 - 45°, 45 - 90°, 90 - 135° and 135 - 180° in Abduction, and the reverse in Adduction).

		Abduction										Adduction									
		DA		DM		DP		MT		Tmax		DA		DM		DP		MT		Tmax	
		Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD
Contralateral	0 - 45°	0,70	1,00	0,62	0,19	0,59	0,12	11,69	2,76	15,95	3,25	0,29	0,23	0,30	0,24	0,36	0,15	5,50	8,17	10,53	10,70
	45 - 90°	0,101	0,18	0,90	0,13	0,85	0,21	7,92	8,11			0,38	0,28	0,43	0,23	0,40	0,17	8,37	9,64		
	90 - 135°	0,67	0,56	0,65	0,54	0,60	0,53	8,31	6,78			0,30	0,36	0,37	0,37	0,28	0,28	6,16	7,31		
	135 - 180°	0,46	0,59	0,39	0,51	0,41	0,64	3,67	5,70			-	-	0,25	0,36	0,24	0,34	2,63	3,89		
	0 - 45°	0,71	0,17	0,71	0,17	0,68	0,24	13,21	6,20	16,99	5,65	0,21	0,22	0,39	0,26	0,29	0,20	2,37	5,01	7,24	11,85
	45 - 90°	0,87	0,37	0,79	0,36	0,71	0,36	10,18	8,59			0,25	0,17	0,38	0,28	0,32	0,21	5,47	10,54		

Ipsilateral	90 - 135°	0,66	0,93	0,40	0,40	0,34	0,36	3,43	6,05			0,12	0,13	0,22	0,27	0,20	0,24	3,82	7,49
	135 - 180°	0,12	0,25	0,14	0,31	0,13	0,33	1,27	3,17			0	0	0,12	0,29	0,32	0,21	0,99	2,98

Table 8 Suppl: Electromyographic results of the Anterior (DA), Middle (DM) and Posterior (DP) portions of the Deltoid Muscle in Group 0, in the Forward Flexion/Extension isokinetic exercise represented by values of mean and Standard Deviation (“SD”). It is also represented the Mean Torque (“MT”) and the Maximum Torque (“Tmax”). Each parameter is evaluated for a specific interval of amplitude (0 - 45°, 45 - 90°, 90 - 135° and 135 – 180° in Forward Flexion, and the reverse in Extension)

		Forward Flexion										Extension									
		DA		DM		DP		MT		Tmax		DA		DM		DP		MT		Tmax	
		Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD
Contralateral	0 - 45°	0,64	0,15	0,65	0,12	0,55	0,24	23,25	10,01	28,45	10,48	0,08	0,03	0,24	0,16	0,41	0,12	16,03	7,71	17,29	32,14
	45 - 90°	0,91	0,18	0,93	0,18	0,87	0,31	26,10	10,88			0,08	0,03	0,23	0,17	0,35	0,14	26,91	10,56		
	90 - 135°	0,90	0,15	0,94	0,19	1,03	0,39	22,38	9,11			0,10	0,04	0,22	0,15	0,28	0,09	26,12	14,08		
	135 - 180°	0,32	0,45	0,45	0,54	0,61	0,82	12,08	14,37			-	-	0,07	0,12	0,12	0,15	11,33	13,07		
Ipsilateral	0 - 45°	0,59	0,19	0,64	0,20	0,63	0,18	10,69	4,60	12,76	3,80	0,09	0,06	0,30	0,30	0,31	0,18	3,04	3,38	6,55	6,56
	45 - 90°	0,76	0,23	0,75	0,27	0,78	0,16	2,05	3,53			0,16	0,09	0,36	0,33	0,32	0,17	4,36	5,87		

90 - 135°	0,15	0,33	0,30	0,41	0,32	0,4 5	0,96	2,16			0,05	0,06	0,11	0,15	0,11	0,15	1,13	2,52
135 - 180°	0	0	0	0	0	0	0	0			0	0	0	0	0	0	0	0

Table 9 Suppl: Electromyographic results of the Anterior (DA), Middle (DM) and Posterior (DP) portions of the Deltoid Muscle in Group 1, in the Forward Flexion/Extension isokinetic exercise represented by values of mean and Standard Deviation (“SD”). It is also represented the Mean Torque (“MT”) and the Maximum Torque (“Tmax”). Each parameter is evaluated for a specific interval of amplitude (0 - 45°, 45 - 90°, 90 - 135° and 135 – 180° in Forward Flexion, and the reverse in Extension).

		Forward Flexion										Extension									
		DA		DM		DP		MT		Tmax		DA		DM		DP		MT		Tmax	
		Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD
Contralateral	0 - 45°	0,69	0,27	0,63	0,25	0,57	0,18	13,04	6,65	18,99	7,92	0,29	0,25	0,43	0,21	0,81	0,65	7,49	7,89	17,32	12,42
	45 - 90°	0,87	0,33	0,79	0,28	0,86	0,28	14,42	9,32			0,26	0,15	0,44	0,20	0,86	0,63	13,45	12,21		
	90 - 135°	0,83	0,55	0,89	0,57	1,00	0,59	11,65	8,71			0,20	0,15	0,35	0,22	0,52	0,32	11,56	12,16		
	135 - 180°	0,41	0,74	0,51	0,77	0,60	0,93	6,61	10,05			-	-	0,22	0,38	0,36	0,61	2,65	4,19		
Ipsilateral	0 - 45°	0,63	0,10	0,71	0,17	0,71	0,24	12,68	5,76	16,49	5,37	0,24	0,28	0,45	0,31	0,56	0,32	2,77	3,80	10,95	11,65
	45 - 90°	0,90	0,21	0,91	0,25	0,93	0,26	9,75	8,90			0,32	0,37	0,48	0,33	0,59	0,34	7,25	9,62		

90 - 135°	0,68	0,43	0,65	0,43	0,71	0,4 7	4,96	6,29			0,18	0,22	0,33	0,33	0,44	0,41	8,57	12,0 8
135 - 180°	0,45	0,47	0,47	0,50	0,47	0,4 9	5,67	5,50			0	0	0,26	0,32	0,33	0,41	5,40	8,26



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Electronic artwork

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